

Transistor mismatch effect on common-mode gain of cross-coupled amplifier

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Abstract

In this paper, the analytical approach of MOS transistor mismatch effect on common-mode gain of cross-coupled amplifier is presented. Transconductance (MOS transistor parameter) mismatch effect on common-mode gain of cross-coupled amplifier was analyzed. This study was started with mathematical derivation for representing the mismatch effect of transconductance between 2 differential pairs of cross-coupled amplifier due to common-mode voltage. The derivation result was simulated based on Monte Carlo simulation with random transconductance mismatch rate from 0.05% until 1%. The common-mode gain increases 36.9 dB and average common-mode gain is -81.1 dB. The transconductance mismatch rate increases followed by increase in common-mode gain. The results can be used by circuit designers to design analog circuits, especially operational amplifier used for biosignals processing to minimize the common-mode gain of their circuits. This research presents aid to circuit designers to improve their circuits performance.

Keywords: biosignals processing, common-mode gain, cross-coupled amplifier, MOS transistor mismatch, transconductance

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1. Introduction

CMOS cross-coupled amplifier is frequently used in various application. For example, Fully Balanced Differential Difference Amplifier (FBDDA) is mainly constructed by using Cross-Coupled Amplifier (CCA) [1-4]. MOS transistor mismatch often happens after fabrication until 3%, depends on the fabrication technology [5]. There are some MOS transistor parameters which can be considered, such as mismatch in mobility, W/L ratio, oxide capacitance and threshold voltage. Furthermore, the W/L ratio corresponds to transconductance (g_m) [6].

As shown in Figure 1, biosignals, such as Electroencephalogram (EEG), Electrooculogram (EOG), Electrocardiogram (ECG), Electromyogram (EMG) are widely used for medical applications and have small amplitude and low frequency. The biosignals amplitude and frequency are in the order of μV to mV and DC to a few kHz, respectively [7-12]. Common-Mode Rejection Ratio (CMRR) is ratio of differential gain and common-mode gain (A_{cm}). As parameter of CMRR, A_{cm} is important to be reduced when main circuit like CCA is applied for biosignals. The smaller the A_{cm} the better the CMRR [13-15].

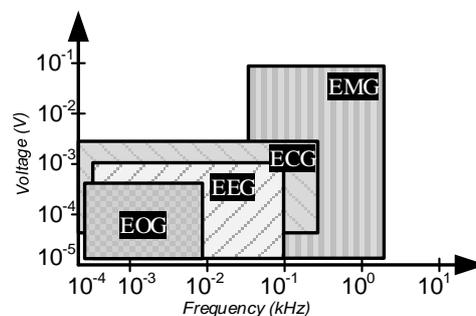


Figure 1. Voltage and frequency ranges of some biosignals

Furthermore, common-mode voltage (V_{cm}) can be caused by power-line interference which normally has frequency of 50Hz or 60 Hz, depends on local power-line frequency. Therefore, the V_{cm} becomes problem for biosignal processing [16-20]. In this paper, study of g_m mismatch effect on A_{cm} of CCA by large signal analysis (mathematical derivation) and simulation is presented. Section 2 discusses the mathematical derivation of circuit analysis of CCA based on the effect of g_m mismatch on its A_{cm} . Section 3 describes simulation results representing g_m mismatch effect on A_{cm} of CCA. Finally, section 4 concludes this study.

2. Transconductance Mismatch Effect on Cross-coupled Amplifier

In some text books and literatures, CCA can be realized as shown in Figure 2 [2], [21, 22]. It consists of 2 differential pairs which matching between MOS transistors is very important to achieve low common-mode gain. In order to simplified the circuit analysis, R_s and R_d are used with well-matched condition. MOS transistor mismatch often occurs due to W/L ratio which is designed by circuit designer [23]. Furthermore, W/L ratio has relationship with g_m as mentioned in (1) [24, 25]. Therefore, the effect of g_m mismatch on 2 differential pairs of CCA is analyzed in this section.

$$\begin{aligned} g_m &= \frac{\partial I_d}{\partial V_{gs}} \\ &= \sqrt{2\mu C_{ox} \frac{W}{L} |I_d| (1 + \lambda V_{ds})} \\ &= \sqrt{2\mu C_{ox} \frac{W}{L} |I_d|} \end{aligned} \quad (1)$$

Firstly, the circuit analysis is started with drain to source current (I_d) definition. Based on large signal analysis, I_d of M_1 - M_4 in Figure 1 can be defined as $I_{di} = g_{mi} V_{gsi}$ $i \in \{1,2,3,4\}$. Giving V_{cm} as the input into gates of the MOS transistors, the I_d of the M_1 - M_4 become

$$I_{d1,2} = g_{m1,2}(V_{cm} - V_a) \quad (2)$$

$$I_{d3,4} = g_{m3,4}(V_{cm} - V_b) \quad (3)$$

current flows through R_s can be defined as follows:

$$I_{d1} + I_{d2} = \frac{V_a}{R_s} \quad (4)$$

$$I_{d3} + I_{d4} = \frac{V_b}{R_s} \quad (5)$$

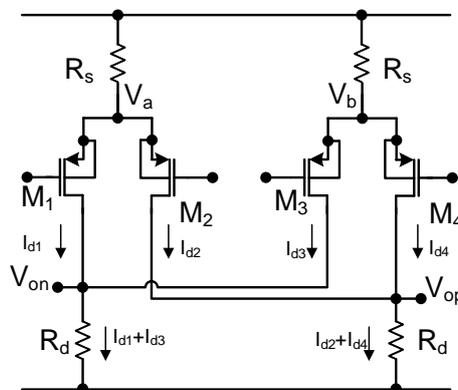


Figure 2. CCA simplified with R_s and R_d

substituting (2–5), V_a and V_b can be derived as follow:

$$V_a = \frac{(g_{m1}+g_{m2})R_s}{(g_{m1}+g_{m2})R_s+1} V_{cm} \quad (6)$$

$$V_b = \frac{(g_{m3}+g_{m4})R_s}{(g_{m3}+g_{m4})R_s+1} V_{cm} \quad (7)$$

on the other hand, V_{op} and V_{on} can be derived as follow:

$$\begin{aligned} V_{op} &= -(I_{d2} + I_{d4})R_d \\ &= -[g_{m2}(V_{cm} - V_a) + g_{m4}(V_{cm} - V_b)]R_d \end{aligned} \quad (8)$$

$$\begin{aligned} V_{on} &= -(I_{d1} + I_{d3})R_d \\ &= -[g_{m1}(V_{cm} - V_a) + g_{m3}(V_{cm} - V_b)]R_d \end{aligned} \quad (9)$$

output voltage (ΔV_{out}) can be calculated as follows:

$$\begin{aligned} \Delta V_{out} &= V_{op} + V_{on} \\ &= [(g_{m1} + g_{m3} - g_{m2} - g_{m4})V_{cm} - (g_{m1} - g_{m2})V_a - (g_{m3} - g_{m4})V_b]R_d \end{aligned} \quad (10)$$

defining ΔV_{cm} as $(V_{cm} + V_{cm})/2$ and mismatched g_{mj} as $g_{mj+1}(1 + \Delta_{j+1}) \mid j \in \{1,3\}$, where Δ_{j+1} is mismatch rate of g_{mj+1} , A_{cm} can be derived as follows.

$$\begin{aligned} A_{cm} &= \frac{\Delta V_{out}}{\Delta V_{cm}} \\ &= \left[g_{m2}\Delta_2 + g_{m4}\Delta_4 - \frac{g_{m2}\Delta_2\alpha R_s}{\alpha R_s+1} - \frac{g_{m4}\Delta_4\beta R_s}{\beta R_s+1} \right] R_d \\ &= \left[g_{m2}\Delta_2 \left(1 - \frac{\alpha R_s}{\alpha R_s+1} \right) + g_{m4}\Delta_4 \left(\frac{\beta R_s}{\beta R_s+1} \right) \right] R_d \end{aligned} \quad (11)$$

Where α and β stand for $g_{m2}(2 + \Delta_2)$ and $g_{m4}(2 + \Delta_4)$, respectively. From the above derivation, the A_{cm} of CCA is proportional to mismatch of g_m . Based on (11), the A_{cm} is finite, so that some amount of V_{cm} may pass through the CCA. If the CCA is applied to enhanced amplifier, the V_{cm} will be amplified and deteriorate performance of the enhanced amplifier.

3. Simulation Result

In this section, the g_m mismatch effect was evaluated using simulations. Referring to (11), the simulations were done based on the condition on Table 1. Well-matched resistors R_s and R_d were given with the value of 100 k Ω and 2 k Ω , respectively. Mismatch rate of both g_{m1} and g_{m2} are set in the range of 0,05% - 1%.

Table 1. Simulation Condition

Variable	Value
R_s	100 k Ω
R_d	2 k Ω
Δ_2, Δ_4	0,05% - 1%

3.1. Effect of Increasing Mismatch Rate to A_{cm}

In this subsection the effect of increasing Δ is considered and in the next subsection the Δ is extended to random condition. Assuming the Δ of both g_{m1} and g_{m2} increase from 0,05% until 1%. Figure 3 shows simulation result based on the increasing Δ . From the simulation result, the A_{cm} increases from -100 dB until -74 dB. It means the A_{cm} increases 26 dB by the increase of Δ about 1%. This means when Δ is getting bigger, so is the A_{cm} .

3.2. Effect of Random Mismatch Rate to A_{cm}

In order to realize the effect of random mismatch rate, Monte Carlo simulation was used. It was done by 500 times with random and different value of Δ_2 and Δ_4 to get data of A_{cm} . Figure 4 shows histogram of the A_{cm} . Because of random Δ_2 and Δ_4 from 0.05% until 1%, the A_{cm} varies from -111.2 dB to -74.3 dB. From 500 random configuration of Δ_2 and Δ_4 values, most of A_{cm} is in the range from -75 dB to -85 dB, therefore average A_{cm} is -81.1 dB. The random mismatch rate from 0.05% until 1% increases A_{cm} 36.9 dB.

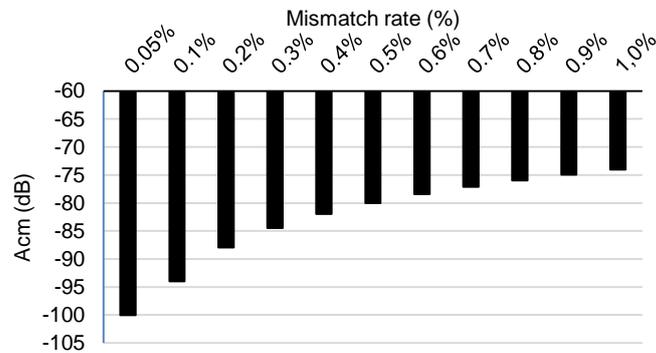


Figure 3. A_{cm} [dB] based on increasing Δ from 0.05% until 1%.

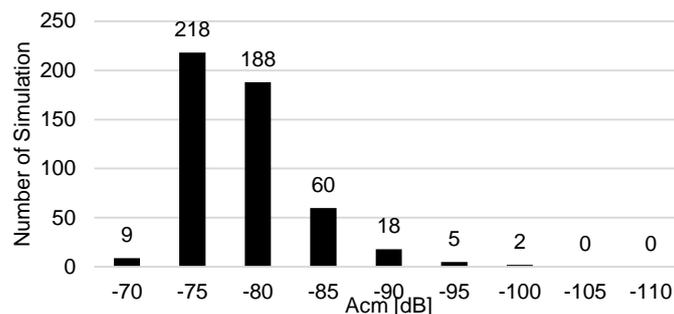


Figure 4. A_{cm} [dB] based on random mismatch rate from 0.05% until 1%.

4. Conclusion

The effect of transistor mismatch on common-mode gain of cross-coupled amplifier has been presented and identified based on mathematical derivation and simulation. The common-mode gain increases along with the increase in transconductance mismatch rate. The results can be used by analog circuit designer to design enhanced operational amplifier with low transistor mismatch effect on common-mode gain.

In the future, mathematical derivation and simulation based on multiple mismatch of MOS transistor parameters such as R_s , R_d , threshold voltage, mobility, and oxide capacitance will be considered in order to represent actual condition. Furthermore, development of common-mode gain reducer and layout technique are also necessary.

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References

- [1] Younghyun Y, Hyungdong R, Jeongjin R. A True 0.4-V Delta-Sigma Modulator Using a Mixed DDA Integrator Without Clock Boosted Switches. *IEEE Transactions on Circuits and Systems II: Express Briefs*. 2014; 61 (4): 229-233.

- [2] Abidin Z, Tanno K, Mago S, Tamura H. A New Instrumentation Amplifier Architecture Based on Differential Difference Amplifier for Biological Signal Processing. *International Journal of Electrical and Computer Engineering*. 2017; 7(2): 759-766.
- [3] Tanaka A, Qin Z, Yoshizawa H. A 0.5-V 85-nW Rail-to-rail Operational Amplifier with a Cross-coupled Output Stage. 2013 IEEE 20th International Conference on Electronics, Circuits, and Systems (ICECS). Abu Dhabi. 2013: 137-140.
- [4] Ghanad MA, Green MM, Dehollain C. Improving Signal to Noise of Current Mode Circuits by A Cross-coupled Current Mirror Topology. *Electronics Letters*. 2014; 50 (13): 928-930.
- [5] Chen Kaiyuan, Chatterjee T, Christensen K, Rosal J, Edwards H. *Atomic Force Probing in Analog MOSFETs*. The 31st International Symposium for Testing and Failure Analysis (ISTFA). California. 2005: 311-315.
- [6] Hajimiri A, Heald R. *Design Issues in Cross-Coupled Inverter Sense Amplifier*. IEEE International Symposium on Circuits and Systems (ISCAS). California. 1998; 6: 311-315.
- [7] Abidin Z, Tanno K, Mago S, Tamura H. *Novel Instrumentation Amplifier Architectures Insensitive to Resistor Mismatches and Offset Voltage for Biological Signal Processing*. The 46th International Symposium on Multiple-Valued Logic (ISMVL). Sapporo. 2016: 194-199.
- [8] Xiaodan Z, Xiaoyuan X, Libin Y, and Yong L. A 1-V 450-nW fully integrated programmable biomedical sensor interface chip. *IEEE J. Solid-State Circuits*. 2009; 44 (4): 1067-1077.
- [9] Webster J. G. *Medical Instrumentation: Application and Design*. Third Edition. New York: Wiley. 1998: 259.
- [10] Chih-Jen Y, Wen-Yaw C, Mely Chen C. Micro-Power Low Offset Instrumentation Amplifier IC Design For Bio-Medical System Applications. *IEEE Transactions On Circuits And Systems-I: Regular Papers*. 2004; 51(4): 691-699.
- [11] Setiawidayat S, Joegijantoro R. Algorithm for the Representation of Parameter Values of Electrocardiogram. *TELKOMNIKA Telecommunication Computing Electronics and Control*. 2018; 16(3): 1295-1302.
- [12] Sada M, Tanno K, Shimoyama M, Abidin Z, Tamura H, Toyama T. *Low Offset Voltage Instrumentation Amplifier by Using Double Chopper Stabilization Technique*. International Conference on Genetic and Evolutionary Computing. Yangon. 2015: 299-309.
- [13] Yu CG, Geiger RL. Nonideality consideration for high-precision amplifiers-analysis of random common-mode rejection ratio. *IEEE Transactions on Circuits and Systems I: Fundamental Theory and Applications*. 1993; 40 (1): 1-12.
- [14] Reza A, Edgar Sanchez-Sinencio. *A biopotential amplifier with improved common mode gain*. 2013 IEEE 4th Latin American Symposium on Circuits and Systems (LASCAS). Cusco. 2013.
- [15] Silverio AA, Chung WY, Tsai Vincent FS. *A low power high CMRR CMOS instrumentation amplifier for Bio-impedance Spectroscopy*. 2014 IEEE International Symposium on Bioelectronics and Bioinformatics (IEEE ISBB 2014). Chung Li. 2014: 1-4.
- [16] Shuo W, Pengju K, Fred CL. Common Mode Noise Reduction for Boost Converters Using General Balance Technique. *IEEE Transactions on Power Electronics*. 2007; 22 (4): 1410-1416.
- [17] Tomasini M, Benatti S, Milosevic B, Farella E, Benini L. Power Line Interference Removal for High-Quality Continuous Biosignal Monitoring With Low-Power Wearable Devices. *IEEE Sensors Journal*. 2016; 16 (10): 3887-3895.
- [18] Bhateja V, Urooj S, Verma R, Mehrotra R. *A Novel Approach for Suppression of Powerline Interference and Impulse Noise in ECG Signals*. International Conference on Multimedia Signal Processing and Communication Technologies (IMPACT 2013). Aligarh. 2013: 103-107.
- [19] Tashev I, Malvar H. S. *Stationary-Tones Interference Cancellation using Adaptive Tracking*. 2007 IEEE International Conference on Acoustics, Speech and Signal Processing - ICASSP 2007. Honolulu. 2007: 201-2014.
- [20] Ramos R, Manuel-Lazaro A, Del Rio J, Olivar G. FPGA-Based Implementation of an Adaptive Canceller for 50/60-Hz Interference in Electrocardiography. *IEEE Transactions on Instrumentation and Measurement*. 2007; 56 (6): 2633-2640.
- [21] Uddin N. and Thiede A. Common Gate Cross-Coupled Differential Amplifier for Near-Field Sensors. *Electronics Letters*. 2008; 45(18): 918 – 920.
- [22] Alzahrer H and Ismail M. A CMOS fully balanced differential difference amplifier and its applications. *IEEE Transactions on Circuits and Systems II: Analog and Digital Signal Processing*. 2001; 48 (6): 614-620.
- [23] Brito JPM. and Bampi S. A DC Offset and CMRR Analysis in a CMOS 0.35 μm Operational Transconductance Amplifier Using Pelgrom's Area/Accuracy Tradeoff. *Microelectronics Journal*. 2009. 40 (9): 1281-1292.
- [24] Allen PE. and Holberg DR. *CMOS Analog Circuit Design*. Second Edition. New York: Oxford University Press. 2002: 88-89.
- [25] Gray PR, Meyer RG. *Analysis and Design of Analog Integrated Circuits*. Fourth Edition. John Wiley & Sons, Inc. 2001: 74.